



# PASSION FOR INNOVATION

# Deep Learning for real-time neural decoding of grasp

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## Background – B-Cratos project

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Applied Data Science: focus on application → context of research in a larger project



The goal is to develop a closed-loop BCI and to validate it with NHPs (Non-Human Primates), with the following technical objectives:

- 1. Proof-of-concept, high-speed, wireless brain implant capable of two-way communication without battery
- 2. General-purpose, high-speed intra-body communications technology (Fat-IBC)
- 3. HPC based ML models deployed on embedded board for low-power inference and control
- 4. Improvements of biomechatronic hand prothesis
- 5. High-resolution sensorized skin

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This project has received funding from the European Horizon 2020 research and innovation programme under GA No 965044





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Partners from 5 countries Coordinated by University of Uppsala



# Neural Decoding for Neuroprosthetics

- Goal: translate the signal from brain implants
   into commands for a prothesis
- Main steps
  - Brain electrodes pick up analogue signals from large neuron populations
  - Post-processing is applied to convert the signal to "spike-trains": multi-channel time series of binary data
  - Decoding algorithm is applied to convert the signal to command for the prothesis





From C. Pandarinath and S. J. Bensmaia, "The science and engineering behind sensitized brain-controlled bionic hands," Physiological Reviews, p. physrev.00034.2020, Sep. 2021 doi: 10.1152/physrev.00034.2020. <u>Edited.</u>





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- Off-line decoding is well understood, real-time decoding is challenging
- State-of-the-art models are simple (e.g., linear models): Patient "learns to drive" the model
  - Also reflects neuroscientist's need for explainability
- Neural signal changes over time and requires daily re-training of models
- B-Cratos aims to improve the overall accuracy of models and to re-use information across sessions
  - · Lower effort for patient, easier adoption, more natural usage
  - Modern machine learning techniques can support this goal









### ML task overview

• Working on a reference dataset

- Focused on a reference dataset provided by a partner (German Primate Center)
- Monkey trained for a grasping task
- Neural recording from multiple cortex regions
- Monkey grasping objects presented in sequence
- Objects grouped by shape and size, presented randomly
- 2 monkeys, 6 recording sessions (i.e., different days)
- Learning Tasks
  - Grasping phase detection
  - Object classification





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### **Dataset structure**

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•••• Recording sessions, trials, metadata

**Recording sessions** 

NHP identifier	Dataset identifier	$\mid \# \text{ Channels}$	$\mid \# \text{ Trials}$
М	MRec40 MRec41 MRec42	$552 \\ 568 \\ 554$	745 757 653
Z	ZRec32 ZRec35 ZRec50	391 388 369	$ \begin{array}{c} 687 \\ 724 \\ 610 \end{array} $







- Each trial discretised in bins of 40ms
- Results in dense matrix
  - channels x time\_bins
  - Each bin contains the number of spikes
- Time stamps associated to a bin
- Each matrix is Associated to object id

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- 1. Classes are de-duplicated (i.e., same object in different groups)
- 2. Dataset is split by trial
  - 1. 80% training + validation, 20% test)
  - 2. stratified by class
- 3. Split is stratified by class
- 4. Under-represented class are removed (i.e., less than 3 trials per session)
- 5. Total of 39 classes left







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#### **Goal: simulate real-time decoding**

- Sliding windows extract sub-sequnces of 12 bins
- Grasp phase classification includes all data labelled with 0 (no grasp) and 1 (grasp)
- Object classification includes only the sub-sequences in the grasp phase, labelled with object ID



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- LSTMs demonstrated good performance in literature
- Started from there (quite naïve in fact)
- **Bidirectionality** proved to be very effective
- Lots of dropout to prevent heavy overfitting
- Hyperparameter optimization

Hyperparameter	Values	Sel	lected		
	(L1=0.01, L2=0.01)	M	Z		
LSTM layers	$ $ { 1, 2, 3, 4 }	2	1		
Hidden units	$\{ 16, 32, 40, 64 \}$	40	40		
Dropout	$\{0, 0.2, 0.4, 0.6, 0.7, 0.8\}$	0.8	0.7		
Kernel regularisation	$\{ \text{ None, L1, L2, L1 + L2} \}$	L2	L2		
Recurrent regularization	$\{ \text{ None, L1, L2, L1 + L2} \}$	L2	L1+L2		
Initial learning rate	$\left  \ \left\{ \ 10^{-3}, \ 2 \cdot 10^{-4}, \ 10^{-4} \  ight\}  ight.$	$  10^{-3}$	$  10^{-3}$		





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- Significant class imbalance here, with no grasp class
   ~10 times more represented than grasp class
- LSTM model reaches an accuracy of at least 98% for all datasets, the F1 score is always greater than 0.95
- Result relevant for a finite-state prosthesis control scenario
  - Each 40ms time step: predict prosthesis status (grasp vs. no-grasp)
  - 1% of unwanted movement for each time step
  - 0.1% of unresponsive prosthesis







(b) Grasping phase detection accuracy metrics.

Dataset id	Accuracy	F1 score
MRec40	99%	0.96
MRec41	99%	0.96
MRec42	99%	0.97
ZRec32	99%	0.96
ZRec35	98%	0.96
ZRec50	98%	0.95









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- Top 1% accuracy ranging from 61% to 74% across different sessions
- Neighbouring classes referred to similar objects
  - Relaxed accuracy defined as misclassification by 1 class (i.e., distance 1 from diagonal)





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0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0
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• • Object classification – comparison with state of the art

Results

Animal	Metric	Present work	Schaffelhofer, 2015	Fabiani, 2021
M	Accuracy	$69.7\pm4\%$	$62.9\pm3.6\%$	n/a
	Accuracy	$62.3\pm1.2\%$	$61.4\pm4.1\%$	n/a
Global	Accuracy Relaxed accuracy	$65.9 \pm 4.9\%$ $94.4 \pm 3.1\%$	$62\% \\ 86.5\%$	$22\% \\ 59\%$

- Schaffelhofer et al. report an average accuracy for the hold phase of 62% over a total of 10 recording sessions (against the six available for this work)
  - Offline naive bayesian classifier applied to the whole hold phase vs. sligding window
  - Validated with a leave-one-out (LOO) approach
  - Dataset fraction used for training was significantly higher
  - Significantly better (M) and slightly better (Z)

accuracy results in a harder set-up. Significantly better relaxed accuracy

- Fabiani reported offline and online accuracy figures
  - This work outperforms both cases, despite the use of similar LSTM architechtures
  - Improvement likely due to bidirectional networks and stronger regularization

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- Real life scenario involves frequent retraining, also during recording sessions
- Neuroscientist's requirement is to limit training to a minimum, and let the model work for most of the time
  - Even more relevant for patients
- Smaller training sets were evaluated
- The model is still outperforming the previous SotA down to 40% of training data

$Training + validation \ set$	Accuracy	Relaxed accuracy
80%	74.1%	98.3%
70%	70.1%	97.1%
60%	69%	93.7%
50%	62.8%	94%
40%	63.8%	92.8%
$30\%^*$	59.2%	87.5%
$20\%^{**}$	51%	81%

 $^{\ast}$  validation is 30% of training set to ensure at least one representative per class

 $^{**}$  validation is 40% of training set







## Remarks and future work

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- LSTM can match and outperform previous approaches on a known dataset
  - More accurate prosthesis control can be enabled by modern architectures, at the expense of some explainability
- Results for relaxed accuracy are very promising for the final application
  - Continuous control of few degrees of freedom (regression on few variables)
  - Finite-state control of 5-6 grasp types (classification on fewer classes)

#### Future work

- Neural data evolves with time: robustness/adaptability of models is key to reduce patients and physicians effort
- Fine-tuning with limited data already proven effective
- Semi-supervised training with usage data is an open problem, inputs from the community are welcome!









### **Thanks for your attention!**

#### Acknowledgments









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